EXPRESS MAIL LABEL NO. EL874429111US DATE OF DEPOSIT: December 17, 2001

JC07 Rec'd PCT/PTO 1 7 DEC 2001

FORM PTO-1390 U.S. DEPAR	TMENT OF COMMERCE PATENT AND TRADEMARK OFFI	CE ATTORNEY'S DOCKET NUMBER		
TRANSMITTAL LETTER TO THE UNITED STATES 5585-61534				
DESIGNATED/ELECTED OFFICE (DO/EO/US) US APPLICATION NO (IF KNOWN, see 37)				
CONCERNING A FILING UNDER 35 U.S.C. § 371 Not 10 / ig 0 1 8 6 0				
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INTERNATIONAL APPLICATION NO INTERNATIONAL FILING DATE PRIORITY DATE CLAIMED 19 June 2000 18 June 1999				
PCT/GB00/02216	19 June 2000	10 0010 1333		
TITLE OF INVENTION BIOLOGICALLY ACTIVE MAT	ERIALS			
APPLICANT(S) FOR DO/EO/US				
Ruth Duncan, Dale Hreczuk-Hirst	and Lisa German to the United States Designated/Elected Office (E	OO/EO/US) the following items and other information.		
1	ubmission of items concerning a filing under 35 U			
_	D or SUBSEQUENT submission of items concer			
	request to begin national examination procedures			
rather than delay of	xamination until the expiration of the applicable	time limit set in 35 U S C		
	Articles 22 and 39(1)	and by the 10th month from the earliest claimed		
4 A proper Demand priority date	for International Preliminary Examination was m	naue by the 19 month from the earnest claimed		
5 🛛 A copy of the Inte	rnational Application as filed (35 U S C § 371(c))(2))		
a ⊠ is transmitte	ed herewith (required only if not transmitted by th	e International Bureau).		
b ☐ has been tra	nsmitted by the International Bureau			
c is not require	red, as the application was filed in the United State	es Receiving Office (RO/US)		
6. A translation of the	A translation of the International Application into English (35 U S C § 371(c)(2))			
7 🛭 Amendments to th	Amendments to the claims of the International Application under PCT Article 19 (35 U S C § 371(c)(3))			
a 🔲 are transmi	a are transmitted herewith (required only if not transmitted by the International Bureau)			
b have been transmitted by the International Bureau				
c have not be	c have not been made, however, the time limit for making such amendments has NOT expired.			
	en made and will not be made			
8 A translation of th	8 A translation of the amendments to the claims under PCT Article 19 (35 U.S.C § 371(c)(3))			
				
10 A translation of th § 371(c)(5))				
Items 11. to 16. below concern document(s) or information included:				
11 🛛 An Information Dis	closure Statement under 37 C F R §§ 1 97 and 1.9	98 `		
	iment for recording A separate cover sheet in co	impliance with 37 C F.R §§ 3 28 and 3 31 and the		
13 🛛 A FIRST prelimina	ry amendment			
☐ A SECOND or SU	BSEQUENT preliminary amendment			
14 A substitute specifi	cation			
15 \(\sum \) A change of power	of attorney and/or address letter			
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EXPRESS MAIL LABEL NO. EL874429111US DATE OF DEPOSIT: December 17, 2001

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17. The following fe				CALC	CULATIONS	(PTO USE ONLY)
BASIC NATIONAL FE	E (37 C.F.R. §§ 1.492(a)(1)-(5)):				
Neither International	Preliminary Examination	fee (37 C.F.R. § 1 482)	\$1,040.00			
International Prelimin USPTO but Internation	nary Examination fee (37 onal Search Report prepare	C.F.R. § 1 482) not paid t red by the EPO or JPO	o \$890.00	1		
but International Sea	rch fee (37 C.F.R. & 1.445	C.F.R. § 1.482) not paid t 5(a)(2)) paid to USPTO as	an			
but all claims did not	satisfy provisions of PC	d to USPTO (37 C.F.R. § 1 Γ Article 33(1)-(4)	\$710.00			
International Prelimi	nary Examination fee paid ed provisions of PCT Arti	d to USPTO (37 C F.R. § icle 33(1)-(4)	1.48 <i>2</i>) 			
	ENTER APPI	ROPRIATE BASIC	FEE AMOUNT =	\$	890.00	
Surcharge of \$130.00	for furnishing the oath or	declaration later than	20 🔲 30	\$		
months from the earlie	est claimed priority date (NUMBER EXTRA	RATE	_		
Total claims	21 - 20 =	1	x \$18.00	\$	18.00	
Independent Claims	3 - 3 =	0	x \$84.00	\$	0.00	
	DENT CLAIM(S) (if appl	licable)	+ \$280.00	\$	0.00	
	TOT	TAL OF ABOVE CA	ALCULATIONS =	\$	908.00	
Reduction of 1/2	for filing by small entity	Small entity status is clair	ned for this application.	\$	0.00	
			SUBTOTAL =	\$	908.00	
Processing fee of \$13	0.00 for furnishing the Er	iglish translation later than	20 30 +	\$	0.00	
Months from the earli	est claimed priority date (TOTAL N	ATIONAL FEE =	\$	908.00	
Fee for recording the	enclosed assignment (37	C.F.R § 121(h)). The ass	signment must be	\$	0.00	
accompanied by an ap	opropriate cover sheet (37	CFR. §§ 3.28, 3 31) \$4	i0.00 per property + ES ENCLOSED =	\$	908.00	
		TOTALTE	ES ENCEOSED		REFUND →	\$
				<u> </u>	CHARGE →	\$
a. A check in the amount of \$908 00 to cover the above fees is enclosed						
b. Please charge my Deposit Account No in the amount of \$ to cover the above fees A duplicate copy of this sheet is enclosed.						
c. The Director is hereby authorized to charge any additional fees that may be required, or credit any overpayment, to Deposit Account No 02-4550. A duplicate copy of this sheet is enclosed						
d. Please return the enclosed postcard to confirm that the items listed above have been received						
NOTE: Where an a or (b)) must	ppropriate time limit un t be filed and granted to	der 37 C.F.R. § 1.494 or restore the application to	§ 1.495 has not been met, a pending status.		to revive (37 (C.F.R. § 1.137(a)
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KLABOUIS	T SPARKMAN, LLP		SIGNATURE William D N		.D.	_
One World	Trade Center, Suite 1600		NAME			
121 S W Sa	llmon Street R 97204-2988		30,878			
Portiand, Or	X 714U4-4700		REGISTRAT	ION NUN	1BER	

cc: Docketing

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17 DEC 2001

IN THE UNITED STATES PATENT AND TRADEMARK OFFICE

In re Application of: Duncan et al.

Application No. Not Yet Assigned

Filed: Herewith

For: BIOLOGICALLY ACTIVE MATERIALS

Examiner: Not Yet Assigned

Date: December 17, 2001

BOX PCT COMMISSIONER FOR PATENTS WASHINGTON, D.C. 20231 Art Unit: Not Yet Assigned

CERTIFICATE OF MAILING

I hereby certify that this paper and the documents referred to as being attached or enclosed herewith are being deposited with the United States Postal Service on December 17, 2001 as U S Express Mail in an envelope addressed to: BOX PCT, Commissioner for Patents, Washington, D.C. 20231.

William D Noonan, M.D., J.D.

Attorney for Applicant

PRELIMINARY AMENDMENT

Prior to examination of the above-referenced application, please amend the application as follows:

In the Specification:

On page 1, line 2, please insert the following:

PRIORITY CLAIM

This is a U.S. National Stage § 371 of PCT/GB00/02216, filed June 19, 2000, which was published in English under PCT Article 21(2), which claims the benefit of U.K. Application GB9914187.1, filed June 18, 1999, and U.K. Application GB9930252.3, filed December 22, 1999.

In the Claims:

Please cancel pending claims 14 and 15 without prejudice. Please amend pending claims 2-13 and 16-23 as follows:

1. (Reiterated) A polymer drug conjugate comprising: at least one anti-cancer agent; and

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a dextrin polymer, wherein said dextrin polymer is modified by succinoylation by at least 20mol% characterised in that the stability of the polymer drug conjugate is enhanced.

- 2. (Amended) The polymer drug conjugate according to Claim 1, wherein said dextrin is succinoylated to at least 30mol%.
- 3. (Amended) The polymer drug conjugate according to Claim 2, wherein said dextrin is succinoylated from 30% to 40mol%.
- 4. (Amended) The polymer drug conjugate according to Claim 3, wherein said dextrin is succinoylated from 32% to 36mol%.
- 5. (Amended) The polymer drug conjugate according to Claim 4, wherein said dextrin is succinoylated to about 34mol%.
- 6. (Amended) The polymer drug conjugate according to Claim 1, wherein a percentage of α -1-6 linkages in the dextrin is less than 10%.
- 7. (Amended) The polymer drug conjugate according to Claim 6, wherein the percentage of α -1-6 linkages in the dextrin is less than 5%.
- 8. (Amended) The polymer drug conjugate according to Claim 1, wherein a molecular weight of the dextrin is in an average molecular weight range 1000-200000.
- 9. (Amended) The polymer drug conjugate according to Claim 8, wherein a molecular weight of the dextrin is in an average molecular weight range 2000-55000.
- 10. (Amended) The polymer drug conjugate according to Claim 1, wherein the dextrin contains more than 15% of polymers of DP greater than 12.

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- 11. (Amended) The polymer drug conjugate according to Claim 10, wherein the dextrin contains more than 50% of polymers of DP greater than 12.
- 12. (Amended) The polymer drug conjugate according to Claim 1, wherein said anti cancer agent is selected from the group consisting of: cyclophosphamide; melphalan; carmusline; methotrexate, 5-fluorouracil; cytarabine; mercaptopurine; anthracyclines; daunorubicin; doxorubicin; epirubicin, vinca alkaloids; vinblastin, vincristine; dactinomycin; mitomycin C; taxol; L-asparaginase; G-CSF; cisplatin; and carboplatin.
- 13. (Amended) A pharmaceutical composition, comprising the polymer drug conjugate according to Claim 1 and a pharmaceutically acceptable diluent, excipient or carrier.
- 14. Please cancel claim 14.
- 15. Please cancel claim 15.
- 16. (Amended) A polymer drug conjugate comprising: at least one biologically active agent; and a dextrin polymer, wherein said dextrin polymer is modified by succinoylation by at least 20mol% characterized in that the stability of the polymer drug conjugate is enhanced.
- 17. (Amended) The polymer conjugate according to Claim 16, wherein said agent is an imaging agent.
- 18. (Amended) The polymer conjugate according to Claim 17, wherein the imaging agent is tyrosinamide.
- 19. (Amended) The polymer conjugate according to Claim 16, wherein said agent is a diagnostic agent.

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- 20. (Amended) The polymer conjugate according to Claim 16, wherein said agent is a targeting agent.
- 21. (Amended) The polymer conjugate according to Claim 20, wherein the targeting agent is biotin.
- 22. (Amended) A method for treating a disease or disorder in an animal subject, comprising: administering to the animal a pharmaceutically effective amount of the polymer drug conjugate according to Claim 1, thereby treating the disease or disorder in the subject.
- 23. (Amended) The method according to Claim 22, wherein said animal is human.

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REMARKS

By this amendment the specification has been changed to reflect prior related applications. No new matter is added by this amendment.

Claims 15 and 16 are cancelled herein without prejudice. Claims 2-13 and 16-23 are amended to correct form or to remove multiple dependencies in order to reduce the filing fee.

No new matter has been added by this amendment. Examination of the subject application is respectfully requested.

CONCLUSION

If any minor matters need to be addressed, the Examiner is invited to contact the undersigned at the telephone number listed below.

Respectfully submitted,

KLARQUIST SPARKMAN, LLP

William D. Noonan, M.D., J.D. Registration No. 30,878

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121 S.W. Salmon Street

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Facsimile: (503) 228-9446

PATENT

Marked-up Version of Amended Claims and Specification Pursuant to 37 C.F.R. §§ 1.121(b)-(c)

In the Specification:

Page 1, line 2, please insert the following:

--PRIORITY CLAIM

This is a U.S. National Stage § 371 of PCT/GB00/02216, filed June 19, 2000, which was published in English under PCT Article 21(2), which claims the benefit of U.K. Application GB9914187.1, filed June 18, 1999, and U.K. Application GB9930252.3, filed December 22, 1999.--

In the Claims:

Please amend the claims as follows:

- 1. (Reiterated) A polymer drug conjugate comprising:
 - at least one anti-cancer agent; and
- a dextrin polymer, wherein said dextrin polymer is modified by succinoylation by at least 20mol% characterised in that the stability of the polymer drug conjugate is enhanced.
- 2. (Amended) [A] The polymer drug conjugate according to Claim 1, wherein said dextrin is succinoylated to at least 30mol%.
- 3. (Amended) [A] The polymer drug conjugate according to Claim 2, wherein said dextrin is succinoylated from 30% to 40mol%.
- 4. (Amended) [A] The polymer drug conjugate according to Claim 3, wherein said dextrin is succinoylated from 32% to 36mol%.

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- 5. (Amended) [A] The polymer drug conjugate according to Claim 4, wherein said dextrin is succinoylated to about 34mol%.
- 6. (Amended) [A] The polymer drug conjugate according to [any of Claims] Claim 1[-5], wherein [the] a percentage of α -1-6 linkages in the dextrin is less than 10%.
- 7. (Amended) [A] The polymer drug conjugate according to Claim 6, wherein the percentage of α -1-6 linkages in the dextrin is less than 5%.
- 8. (Amended) [A] The polymer drug conjugate according to [any of Claims] Claim 1₂[-7] wherein [the] a molecular weight of the dextrin is in [the] an average molecular weight range 1000-200000.
- 9. (Amended) [A] The polymer drug conjugate according to Claim 8, wherein [the] a molecular weight of the dextrin is in [the] an average molecular weight range 2000-55000.
- 10. (Amended) [A] The polymer drug conjugate according to [any of Claims] Claim 1[-9], wherein the dextrin contains more than 15% of polymers of DP greater than 12.
- 11. (Amended) [A] The polymer drug conjugate according to Claim 10, wherein the dextrin contains more than 50% of polymers of DP greater than 12.
- 12. (Amended) [A] The polymer drug conjugate according to [any of Claims] Claim 1[-13], wherein said anti cancer agent is selected from the group consisting of: cyclophosphamide; melphalan; carmusline; methotrexate, 5-fluorouracil; cytarabine; mercaptopurine; anthracyclines; daunorubicin; doxorubicin; epirubicin, vinca alkaloids; vinblastin, vincristine; dactinomycin; mitomycin C; taxol; L-asparaginase; G-CSF; cisplatin; and carboplatin.

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- 13. (Amended) A pharmaceutical composition, comprising [a] the polymer drug conjugate according to [any of Claims] Claim 1[-12] and a pharmaceutically acceptable diluent, excipient or carrier.
- 14. Please cancel claim 14.
- 15. Please cancel claim 15.
- 16. (Amended) A polymer drug conjugate comprising:
 - [i)] at least one biologically active agent; and
- [ii)] a dextrin polymer, wherein said dextrin polymer is modified by succinoylation by at least 20mol% characterized in that the stability of the polymer drug conjugate is enhanced.
- 17. (Amended) [A] The polymer conjugate according to Claim 16, wherein said agent is an imaging agent.
- 18. (Amended) [A] The polymer conjugate according to Claim 17, wherein the imaging agent is tyrosinamide.
- 19. (Amended) [A] The polymer conjugate according to Claim 16, wherein said agent is a diagnostic agent.
- 20. (Amended) [A] The polymer conjugate according to Claim 16, wherein said agent is a targeting agent.
- 21. (Amended) [A] The polymer conjugate according to Claim 20 wherein the targeting agent is biotin.
- 22. (Amended) A method [of treatment of] <u>for treating a disease or disorder in</u> an animal subject, [the method including the administration of] <u>comprising</u>:

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administering to the animal a pharmaceutically effective amount of the polymer drug conjugate according to [any of Claims] Claim 1[-12], thereby treating the disease or disorder in the subject.

23. (Amended) [A] The method [of treatment] according to Claim 22, wherein said animal is human.

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BIOLOGICALLY ACTIVE MATERIALS

Field of Invention

This invention relates to biologically active materials and, in particular, to materials 5 which comprise a biodegradable polymer linked to a biologically active agent. The invention is concerned with materials known as polymer-drug conjugates which typically contain a therapeutic agent for instance, a bioactive cytotoxic drug, linked to a polymer back-bone. The linkage between the polymer and the drug is typically by covalent bonding. However, the invention is applicable to other polymer conjugates 10 including those where the biologically active agent is an imaging agent, such as tyrosinamide, a diagnostic agent, or a targeting agent such as biotin.

Reference will be made hereinbelow to polymer-drug conjugates in which the drugs are anticancer agents. However, the present invention has application in connection with other drugs and/or bioactive agents.

Background of the Invention

20 In designing a polymer-drug conjugate, the aim is to deliver a drug effectively to a therapeutic site such as a tumour. It is known, for instance, that polymer-drugs given intravenously can accumulate selectively in solid tumour tissue by the EPR effect.

The most commonly used anticancer agents are low molecular weight compounds which readily gain access to cells by rapid passage across the cell membrane. After intravenous (IV) administration, a large percentage of the injected dose leaves the circulation within a few minutes, resulting in a ubiquitous body distribution of drug and little selective concentration in tumour tissue. By creating a macromolecular polymer-anticancer drug conjugate, there is provided an opportunity to improve tumour specific targeting, to minimise drug entry into sites of toxicity, to control precisely the rate of drug liberation at the target site (giving opportunities for long-

term controlled release) and to deliver the active principal intracellularly, thereby providing a means to overcome p-glycoprotein related multidrug resistance.

Numerous polymers have been proposed for synthesis of polymer-drug conjugates including polyaminoacids, polysaccharides such as dextran, and synthetic polymers such as N-(2-hydroxypropyl)methacrylamide (HPMA) copolymer. However, these polymers have limitations. For example, a dextran-doxorubicin conjugate has been tested clinically and been found to be much more toxic than the parent drug. Furthermore the HPMA copolymers which have been clinically tested have the disadvantage of being non-biodegradable in the main chain.

WO-A-98/56424 discloses a polymer-drug conjugate in which the polymer is the polysaccharide dextrin. Such a polymer-drug conjugate may be prepared in various ways. One method involves succinoylating dextrin and reacting the succinoylated dextrin with the drug or a reactive derivative thereof.

WO-A-98/56424 includes an example in which the extent of succinoylation of dextrin varies from 2.26 to 6.64 Mol%. In a further example the drug doxorubicin is conjugated to succinoylated dextrins in which the extent of succinoylation varies from 0.5 to 14.9 Mol%.

WO-A-98/56424 also includes examples showing the rate of degradation of dextrin both in the absence and in the presence of appropriate enzymes and also in rat plasma.

For at least certain applications the rate of degradation of dextrin in a dextrin-drug conjugate is an important consideration. For instance, it may be desirable to have a relatively slow rate of degradation in some applications while in other applications a faster rate of degradation is either acceptable or indeed even preferred.

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Statement of Invention

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It has now been surprisingly discovered that the rate of dextrin degradation is highly dependent on the degree of dextrin backbone substitution. As a result, it is possible to tailor the dextrin by appropriate substitution of its backbone in order to achieve a desired rate of degradation.

According to a first aspect of the invention there is provided a polymer drug conjugate comprising:

- 10 i) at least one anti-cancer drug; and
 - ii) a dextrin polymer characterised in that said dextrin polymer is modified by the addition of pendent

groups so that the stability of the polymer drug conjugate is enhanced.

- The term "dextrin" means a glucose polymer which is produced by the hydrolysis of starch and which consists of glucose units linked together by means mainly of alpha-1,4 linkages. Typically dextrins are produced by the hydrolysis of starch obtained from various natural products such as wheat, rice, maize and tapioca. In addition to alpha-1,4 linkages, there may be a proportion of alpha-1,6 linkages in a particular dextrin, the amount depending on the starch starting material. Since the rate of biodegradability of alpha-1,6 linkages is typically less than that for alpha-1,4 linkages, for many applications it is preferred that the percentage of alpha-1,6 linkages is less than 10% and more preferably less than 5%.
- Any dextrin is a mixture of polyglucose molecules of different chain lengths. As a result, no single number can adequately characterise the molecular weight of such a polymer. Accordingly various averages are used, the most common being the weight average molecular weight (Mw) and the number average molecular weight (Mn). Mw is particularly sensitive to changes in the high molecular weight content of a polymer whilst Mn is largely influenced by changes in the low molecular weight of the polymer.

It is preferred that the Mw of the dextrin is in the range from 1,000 to 200,000, more preferably from 2,000 to 55,000.

The term 'degree of polymerisation' (DP) can also be used in connection with polymer mixtures. For a single polymer molecule, DP means the number of polymer units. For a mixture of molecules of different DP's, weight average DP and number average DP correspond to Mw and Mn. In addition DP can also be used to characterise a polymer by referring to the polymer mixture having a certain percentage of polymers of DP greater than a particular number or less than a particular number.

It is preferred that, in the dextrin-drug conjugate of the present invention, the dextrin contains more than 15 % of polymers of DP greater than 12 and, more preferably, more than 50% of polymers of DP greater than 12.

Modifications to dextrin may be negatively charged groups, neutral groups or positively charged groups, (eg quaternary ammonium groups).

In a further preferred embodiment of the invention said dextrin modification is succinoylation.

In a yet further preferred embodiment of the invention said dextrin succinoylation is greater than 20 mol %. Preferably said dextrin succinoylation is at least 30mol%.

25 More prefereably still said succinoylation is from 30% to 40%.

More preferably still said succinoylation is 30mol%; 31mol%; 32mol%; 33mol%; 34mol%; 35mol%; 36mol%; 37mol%; 38mol%; 39mol%; 40mol%. Ideally said succinoylation is 34mol%.

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In a yet further preferred embodiment of the invention said succinoylated dextrin comprises an anti-cancer agent selected from: cyclophosphamide; melphalan; carmusline; methotrexate, 5-fluorouracil; cytarabine; mercaptopurine; anthracyclines; daunorubicin; doxorubicin; epirubicin; vinca alkaloids; vinblastin; vincristine; dactinomycin; mitomycin C; taxol; L-asparaginase; G-CSF; cisplatin; carboplatin.

More preferably still said anti-cancer agent is doxorubicin.

According to a further aspect of the invention there is provided a pharmaceutical composition comprising a polymer drug conjugate according to any previous aspect or embodiment of the invention.

In a preferred embodiment of the invention said composition comprises a diluent, carrier or excipient.

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In a further preferred embodiment of the invention said polymer drug conjugate is for use in the manufacture of a medicament for the treatment of cancer.

According to a further aspect of the invention there is provided a method to treat an animal, ideally a human being, suffering from cancer by administration of the polymer drug conjugate according to the invention.

It has been found that, in the case of substitution of the dextrin backbone by succinoylation, relatively rapid degradation takes place at a degree of succinoylation of up to about 15%. By contrast a degree of succinoylation above 30% very markedly reduces the rate of degradation.

The present invention provides a dextrin-drug conjugate in which the degree of substitution of the dextrin chain is greater than 15%, more preferably greater than 20% and most preferably greater than 30%.

The drug of the dextrin-drug conjugate may be loaded on the polymer via a linking group, such as succinoyl, in which case it may be attached to some or all of the linking groups. Alternatively the drug may be directly loaded onto the dextrin backbone in which case the drug itself acts as the substituting group. As a further possibility the drug may be loaded partly via a substituting group and partly directly onto the dextrin backbone.

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An embodiment of the invention will now be described by example only and with reference to the following tables and figures;

Table 1 represents the characteristics of different batches of succinoylated dextrin doxorubicin conjugates;

Table 2 shows the anticancer activity of succinoylated dextrin doxorubicin conjugates;

Figure 1 is a graphical representation of the degradation of dextrin, succinoylated dextrin and a succinoylated dextrin doxorubicin conjugate (5% succinoylation, 6% doxorubicin);

Figure 2 is a graphical representation of the degradation of hyper-succinoylated dextrin doxorubicin(34% succinoylation) conjugate with time;

Figure 3 is a graphical representation of the preferential accumulation of succinoylated dextrin doxorubicin conjugate compared to an unconjugated control;

Figure 4 illustrates the effect of the degree of dextrin succinoylation on biodistribution of ¹²⁵I-labelled Dextrin at 34mol% after i.v. administration;

Figure 5 illustrates a comparison of the 1 and 34 mol% modified ¹²⁵I-labelled dextrin at 5 min post i.v administration;

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Figure 6 illustrates a comparison of the 1 and 34 mol% modified ¹²⁵I-labelled dextrin at 1hr post i.v administration; and

Figure 7 represents the presence of ¹²⁵ I –labelled dextrin in the peritoneal wash after i.p. administration at 1hr

Detailed description of the invention

10 Example 1

Dextrin (Mw 51,000 Da) was succinoylated using a modification of the method described by Bruneel *et al* (Polymer, 35 (12),(1994), 2656-2658). Doxorubicin was then conjugated directly via an amide bond, conjugated via an N-cis-aconityl spacer or conjugated via a glycyl-N-cis-aconityl spacer.

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Polymer degradation (unmodified dextrin, succinoylated dextrin (5, 15 mol %) and conjugate) was measured in the presence of amylase or lysosomal enzymes to monitor either changes in polymer molecular weight (GPC) or doxorubicin release (HLPC).

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The dextrin-doxorubin conjugates had a doxorubicin loading of 6-12 wt% dependent on the reaction conditions used and the degree of succinoylation of the dextrin intermediate. Table 1 shows the characteristics of several batches of dextrin-succ-doxorubicin.

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Table 1 Characteristics of batches of dextrin-succ-doxorubicin

Batch No	Dox (wt%)	Free Dox (% total Dox)
1	11.7	0.8
2	11.9	2.0
3	8.7	1.2
4	8.4	0.1



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After a 180 min incubation with amylase, unmodified dextrin is almost completely degraded to low molecular products, whilst the succinoylated dextrin (5 and 15 mol %) and dextrin-succ-doxorubicin show a biphasic pattern of degradation giving rise to fragments of Mw 4,000, 9,500 and 6,400 Da respectively. Unmodified dextrin had a t_{1/2} (time for mass to reach half of its original) of 20 min, succinoylated dextrin and dextrin-succ-doxorubicin a t_{1/2} of approximately 15 min.

Example 2

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In this example the degradation of dextrins of different degrees of modification was compared. The results are shown in Figure 1. It will be seen that native dextrin is rapidly degraded as are also dextrin with 5% succinoylation (whether with or without 6% Dox) and dextrin with 15% succinoylation. However, if dextrin is 34% succinoylated the degree of degradation is markedly less, there being zero% reduction of the peak mass of primary peak after 60 minutes and only 20% reduction after 180 minutes. In addition, Figure 2 shows that 34% succinoylated dextrin doxorubicin conjugate is similarly stable over an extended time course when compared to unconjugated or low level succinoylated (5%) controls.

20 Example 3

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3.

In this example increased uptake of 34% succinoylated dextrin-doxorubicin by tumour cells is shown. Male C57 were injected with 10⁶ B16F10 murine melanoma cells subcutaneously with either doxorubicin hydrochloride or dextrin- succinoyldoxorubicin (34 mol % succinoylation, 11.8% doxorubicin) at 5mg/kg doxorubicin equivalence into the intrapertinoneal cavity (i.p.).

The mice were then culled after 2, 5, and 30 mins and after 1, 2, 5, 24, and 48 hours. Tumours were removed and weighed. The tumour was then homogenised and doxorubicin extracted and quantified by HLPC for total doxorubicin present, Figure

Figure 3 shows there is approximately a three fold increase in tumour levels of doxorubicin were found for the conjugate for all time intervals from 2 min up to 24 hours. After this period, there is no difference between conjugate or the free drug. The elevated levels of the conjugate were at their highest 5 min after injection.

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Example 4

In this example the pharmacology of succinolyated dextrin doxorubicin is determined and is presented in Table 2. Twenty four C57 black mice were injected subcutaneously (s.c.) with 10⁵ B16F10 murine melanoma cells as described above and then monitored daily for well-being and the presence of palpable tumours. When the tumours were palpable, mice were randomly assigned into groups of six and their tumours measured with a micrometer gauge. Tumour size and mouse body weight is recorded. Each group is then injected intra-peritoneally with either sterile saline (negative control), free doxorubicin (5mg kg⁻¹) in sterile saline or dextrindoxorubicin (11.8 wt%, 34% succinolyation) at either 5mg kg⁻¹ or 10mg kg⁻¹, on days 0,1 and 2. The mice were monitored daily and tumour size and body weight recorded. Once the tumour area exceeded 2.89 cm² the mice were culled according to UKCCCR guidelines. Mouse survival is then expressed as % T/C (test/control saline).

The animals treated with doxorubicin (5mg kg-1) displayed a drop in body weight consistent with toxicity. However all mice tolerated the dextrin –doxorubicin conjugate at both doses. The higher dose (10mg kg-1) equates to approximately 2 mg of conjugate. As shown in Table 2, dextrin- doxorubicin conjugate resulted in a T/C of approximately 140% indicating anticancer activity. In contrast, free doxorubicin was not active in this experiment.

Example 5

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The tumour model used was B16F10 murine melanoma. Viable tumour cells (10⁵) were injected subcutaneously into C57/BL mice near the base of the neck. When

tumours were visible 125 I-labelled dextrin (100μ l, 5×10^5 (cpm) was injected i.v. into the tail vein and the mice were culled at 5 min and 1h. A blood sample was taken and the mouse weighed. The major organs were removed and homogenised in a known volume of DI water. Samples (3×1 ml) of each tissue were taken and assayed radioactivity. The total amount of radioactivity per organ was expressed as the percentage of the injected dose or as percent of the dose injected per gram of organ.

Figure 4 shows the effect of the degree of dextrin succinoylation on biodistribution of ¹²⁵I-labelled Dextrin at 34mol% after i.v. administration. Over time it can be noted that there is an decrease in the overall % recovery of the injected dose. Example of organ recoveries, tumour levels increased from 2.5% dose (5 min) to 7.3% dose (1h). Liver levels increased from 10.8% dose (5min) to 11.5% dose (1h) and spleen levels increased from 5.5% dose (5 min) to 9.7% dose (1h). All of the other organs showed a decrease in the % recovery.

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Example 6

Figure 5 shows a comparison of the 1 and 34 mol% modified ¹²⁵I-labelled dextrin at 5 min. At five minutes the overall recovery is greatest in the 34mol%, the tumour % recovery rose from 0.6% dose to 2.5% dose after an increased succinoylation and there was over a two fold difference in the other major organs except the kidney where the % recovery dropped from 15.7% to 11.5% of the injected dose.

Example 7

Figure 6 shows a comparison of the ¹²⁵I-labelled dextrin at 1h. At 1h the accumulation in the kidneys is greater than at 1mol% modified dextrin the 34mol% giving 7.3% dose. The overall recovery for both mol% modified dextrin has decreased over time.

Example 8

Figures 7 show comparisons of recovery in the i.p. wash in the tumour bearing mice. The dextrin at 34mol% is being retained in the i.p. cavity for longer than the other modified polymers

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- 1. A polymer drug conjugate comprising:
 - i) at least one anti-cancer agent; and
 - ii) a dextrin polymer, wherein said dextrin polymer is modified by succinovlation by at least 20mol% characterised in that the stability of the polymer drug conjugate is enhanced.
- A polymer drug conjugate according to claim 1, wherein said dextrin is succincylated to at least 30mol%.
- 10 3. A polymer drug conjugate according to Claim 2, wherein said dextrin is succincylated from 30% to 40mol%.
 - A polymer drug conjugate according to Claim 3, wherein said dextrin is succincylated from 32% to 36mol%.
 - 5. A polymer drug conjugate according to Claim 4 wherein said dextrin is succinoylated to about 34mol%.
- A polymer drug conjugate according to any of Claims 1-5 wherein the
 percentage of α-1-6 linkages in the dextrin is less than 10%.
 - A polymer drug conjugate according to Claim 6 wherein the percentage of α
 1-6 linkages in the dextrin is less than 5%.
- 8. A polymer drug conjugate according to any of Claims 1-7 wherein the molecular weight of the dextrin is in the average molecular weight range 1000-200000.
- 9. A polymer drug conjugate according to Claim 8 wherein the molecular weight of the dextrin is in the average molecular weight range 2000-55000.
 - A polymer drug conjugate according to any of Claims 1-9 wherein the dextrin

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contains more than 15% of polymers of DP greater than 12.

- 11. A polymer drug conjugate according to Claim 10 wherein the dextrin contains more than 50% of polymers of DP greater than 12.
- 12. A polymer drug conjugate according to any of Claims 1-13, wherein said anti-cancer agent is selected from the group consisting of: cyclophosphamide; melphalan; carmusline; methotrexate, 5-fluorouracil; cytarabine; mercaptopurine; anthracyclines; daunorubicin, doxorubicin; epirubicin; vinca-alkaloids; vinblastin; vinca-alkaloids; vinblastin; carboplatin
- 13. A pharmaceutical composition comprising a polymer drug conjugate according to any of Claims 1-12.
- 14 A pharmaceutical composition according to Claim 13 wherein said composition comprises a diluent, carrier or excipient.
- 15. The use of a polymer drug conjugate according to any of Claims 1-12 for the manufacture of a medicament for the treatment of cancer.
 - 16. A polymer drug conjugate comprising:
 - i) at least one biologically active agent; and
- ii) a dextrin polymer, wherein said dextrin polymer is modified by succinculation by at least 20mol% characterised in that the stability of the polymer drug conjugate is enhanced.
 - A polymer conjugate according to Claim 16 wherein said agent is an imaging agent.
 - 18. A polymer conjugate according to Claim 17 wherein the imaging agent is tyrosinamide.

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- 19. A polymer conjugate according to Claim 16 wherein said agent is a diagnostic agent;
- 5 20. A polymer conjugate according to Claim 16 wherein said agent is a targeting
 - 21. A polymer conjugate according to Claim 20 wherein the targeting agent is biotin.

- 22. A method of treatment of an animal subject the method including the administration to the animal a pharmaceutically effective amount of the polymer drug conjugate according to any of Claims 1-12.
- 15 23. A method of treatment according to Claim 22 wherein said animal is human.

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TABLE 2

Compound	Dose mg kg ⁻¹ (day 0,1,2)	Days survival after treatment (mean ± SD)	T/C (%)	Toxic deaths
Control (saline)	-	4.3± 0.5	100	0/6
doxorubicin	5	4.5 ± 0.5^{ns}	103	0/6
Dextrin-Dox	5	6.2 ±0.8°	142	0/6
Dextrin -Dox	10	6.0 ±1.1	138	0/6

N=6 ns = not significant p = 0.0004 p = 0.005



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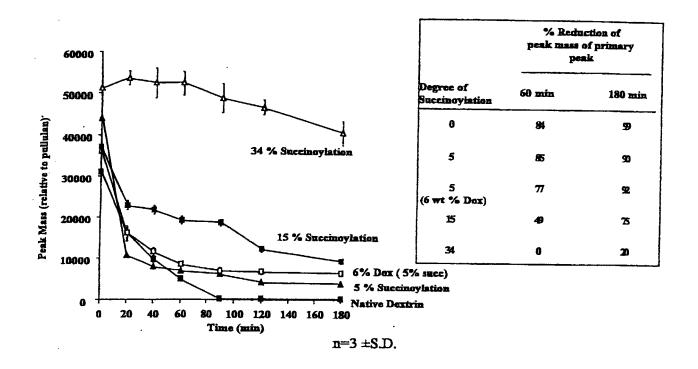


Figure 1 1/6

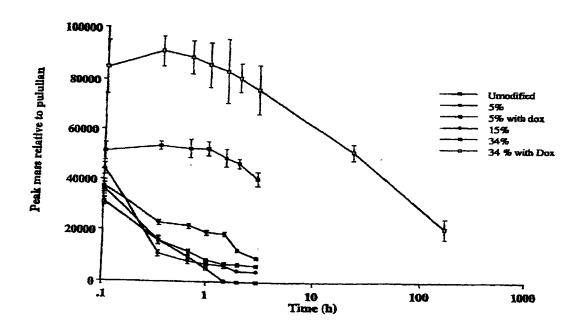


Figure 2 2/6

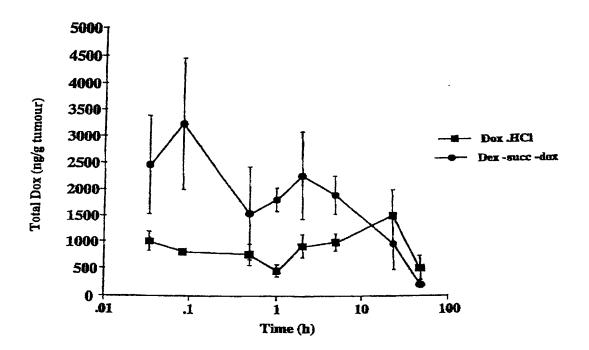
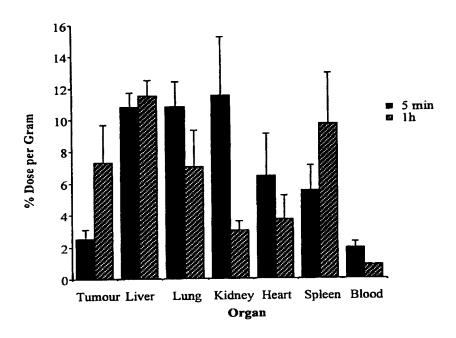
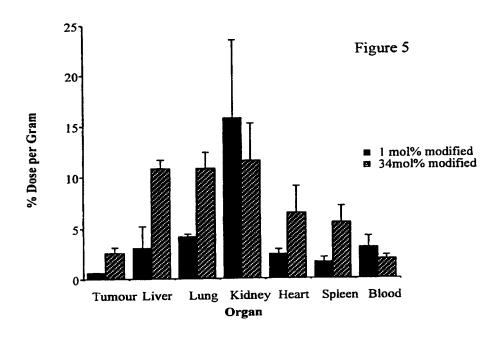


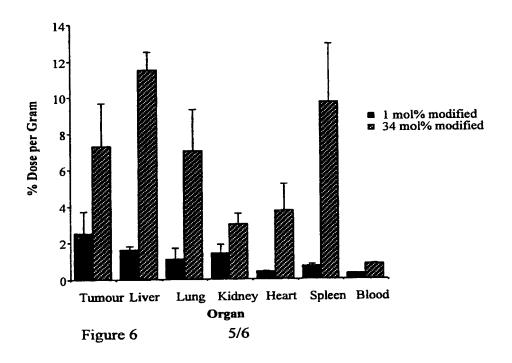
Figure 3 3/6



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Figure 4





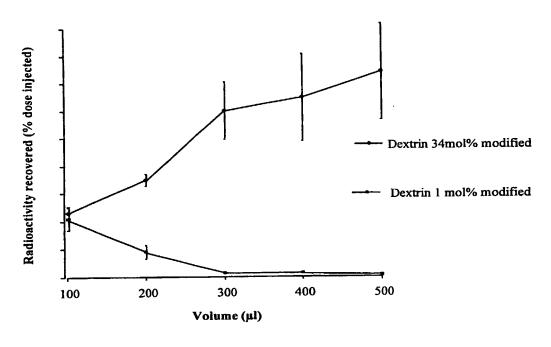


Figure 7.

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My residence, post office address and citizenship are as stated below next to my name,

I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint inventor (if phiral names are listed below) of the subject matter which is claimed and for which a patent is sought on the invention entitled BIOLOGICALLY ACTIVE MATERIALS, the specification of which

	is attached hereto.		_		
×	was filed on December 17	2001 as United Sta	ates Patent Application No. 10/01	<u>8,608</u> .	
\boxtimes	was described and claimed in PCT International Application No. <u>PCT/GB00/02216</u> , filed on 19 June 2000, and as amended under PCT Articles 19 on (if applicable).				
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PCT/GB00/02216	19 June 2000	Pending
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